

1 **Title:**

2 **Electromyographic Activity of selected Trunk, Core, and Thigh Muscles in commonly**
3 **used Exercises for ACL Rehabilitation**

4 **Authors:**

5 Omid A Khaiyat (MD, PhD)

6 Jessica Norris (BSc)

7 School of Health Sciences, Liverpool Hope University

8 Hope Park, Liverpool L16 9JD, UK

9 Tel: 0044 151 291 3262

10 **Corresponding Author:**

11 Dr Omid A Khaiyat

12 Email: alizado@hope.ac.uk

13 **ABSTRACT**

14 **Purpose:** Most of rehabilitation programmes for Anterior Cruciate Ligament (ACL) injury focus
15 on quadriceps-hamstrings activation imbalances and less is known about kinetically linked
16 muscles. Study investigated electromyographic activity of selected trunk, core, and thigh
17 muscles during common rehabilitation exercises for ACL injury.

18 **Subjects and Methods:** Twelve active female volunteers participated in this cross-sectional
19 laboratory study. Surface EMG was used to compare activation of eight trunk, hip/core, and
20 lower limb muscles: Erector Spinae (ES), Rectus Abdominis (RA), Gluteus Maximus (GM),
21 Vastus Lateralis (VL), Rectus Femoris (RF), Vastus Medialis (VM), Biceps Femoris (BF), and
22 Semitendinosus (ST) during Forward Lunge, Double Leg Raise, Glute Bridge, Sit-Up, and
23 Squat.

24 **Results:** Forward lunge produced significantly higher activation in the VM (61.1 ± 19.4), VL
25 (59.2 ± 12.9), and RF (32.0 ± 2.6). Double leg raise generated highest activity in the RF (26.6 ± 2.8)
26 and RA (43.3 ± 4.4); and Glute Bridge in the GM (44.5 ± 19.0) and BF (22.4 ± 4.3). Sit-up produced
27 the highest activation in the RF (36.6 ± 4.7) followed by RA (18.9 ± 3.8). Squat produced a higher
28 activation in VL (55.0 ± 12.9), VM (51.5 ± 18.2), and ES (40.4 ± 18.3).

29 **Conclusion:** Study provide further evidence for developing training programmes for ACL injury
30 prevention and rehabilitation. A combination of exercises to reinstate quadriceps-hamstrings
31 activation balance and enhance core stability is recommended.

32 **Keywords:** Electromyography; Activation Balance; Neuromuscular Function

33 INTRODUCTION

34 The anterior cruciate ligament (ACL) is a common site for sport injury often occurring during a
35 non-contact twisting movement such as pivoting once slowing down or landing¹). ACL injury
36 involves 20% of all sports-related knee injuries with an annual incidence of 81 injuries per
37 100,000 people leading to functional deficits and knee joint instability during sporting
38 activities²). Female athletes are 5.4 to 7.8 times more likely to sustain ACL injury than male
39 athletes³). Increased Q angle and higher joint laxity in females have been linked to abnormal
40 knee kinematics by means of inward rotation of the tibia and placing high levels of stress on the
41 ACL⁴). In terms of neuromuscular characteristics, imbalanced hamstring-to-quadriceps strength
42 and activation ratios have been suggested as potential risk factors in female athletes^{5,6}).

43 Electromyography (EMG) is widely used in the field of sports medicine for investigating
44 potential alterations in the muscle activation patterns in pathologic conditions in order to
45 facilitate the development of evidence-based training and rehabilitation programmes. EMG has
46 however produced conflicting reports regarding ACL injuries: “Quadriceps impairment, as
47 assessed by EMG, has been reported by some researchers while others have reported no
48 impairment⁷⁻⁹). Likewise for hamstrings, despite reports of increased activity in ACL injury,
49 some others found no difference in their activity between patients and controls⁷⁻⁹). Recently,
50 gathering knowledge suggests that altered quadriceps and hamstrings activation in ACL injury
51 may only exist in the presence of knee instability as part of an adaptation strategy to support
52 joint stability i.e. inhibited quadriceps activity with concurrent increased activity of both
53 quadriceps and hamstrings⁹).

54 Deficits within the muscular function (strength and activation) are commonly associated with
55 knee instability in ACL injury leading to the altered joint biomechanics and development of
56 aberrant movement patterns. Quadriceps weakness, in particular, has been associated with these
57 alterations and strength deficits reported between 5%-30%^{5,10}). It has been reported that
58 disproportionate activity of the quadriceps and hamstring muscles results in muscle imbalance
59 and increased strain over the ACL. Appropriate hamstrings activity is essential to counterbalance

60 quadriceps contraction in order to constrain anterior displacement of the tibia^{5,11}). Hence, many
61 ACL injury prevention and rehabilitation programmes attempt to reinstate quadriceps-
62 hamstrings activation balance¹²).

63 In addition to quadriceps and hamstrings, kinetically and functionally linked muscles such as
64 gluteus maximus, rectus abdominis, and erector spinae may also be affected following ACL
65 injury as a result of coping strategies. The gluteus maximus contributes greatly to the core
66 stability, postural alignments, and functional abilities essential for normal gait. Weakness of this
67 muscle may lead to abnormal gait cycle and affect the movement mechanics at both hip and knee
68 joints^{13,14}). It is suggested that gluteus muscle weakness contributes to ACL injury due to
69 increased hip internal rotation and adduction as well as the dynamic knee valgus movements
70 which in turn place additional stress on the knee joint^{1,5}). Rectus abdominis and erector spinae
71 contribute to the core stability and to the controlling of trunk posture during whole-body sports
72 activities¹⁵). It has been reported that enhanced activity of rectus abdominis and erector spinae
73 during stability-enhancing exercise programmes leads to significant enhancement in cooperative
74 spine/core muscle activity and stability¹⁶). Furthermore, both rectus abdominis and erector spinae
75 contribute to the normal gait by generating and controlling the motion between the trunk and
76 pelvis^{17,18}). Hence sufficient activation of these muscles is important in decreasing body's
77 vertical displacement (involving knees) and producing a smoother trajectory for the centre of
78 mass during the gait cycle¹⁷).

79 Both closed and open kinetic chain exercises (CKC and OKC, respectively) are commonly
80 recommended for rehabilitation of ACL injury with a primary focus on restoring normal range
81 of motion and strengthening selected lower extremity and core muscle groups and reducing
82 anterior-posterior (A-P) tibial displacement. Due to weight-bearing nature of CKC exercises a
83 compressive joint load is produced which in turn forces the articular surfaces together in order
84 to eliminate anteroposterior displacement of the tibia relative to the femur⁸). It is suggested that
85 CKC exercises are more effective in enhancing knee arthrokinematics than OKC exercises by
86 means of producing a smaller magnitude of anterior tibial translation and enhance activation of

87 lower extremity muscles (hamstrings-quadriceps in particular) to support knee stability^{8,19}.
88 Hence, it is important to explore exercises with an optimal effect on the restoration of
89 hamstrings-quadriceps activation balance.

90 While the majority of ACL injury prevention and rehabilitation programmes aim to concurrently
91 activate hamstrings and quadriceps to constrain tibial translation, there is limited data on the
92 activity of selected core and trunk muscles during such exercises as the majority of previous
93 studies primarily examined lower extremity (i.e. thigh) muscle activations. With a kinetic chain
94 approach, the present study aimed to investigate activity of selected lower extremity, hip/core,
95 and trunk muscles contributing to the knee joint stability and mobility during five commonly
96 prescribed exercises for ACL injury to provide rationalised evidence-based recommendations.
97 Considering that commonly used therapeutic exercises would have different impact on core and
98 lower extremity muscle activations, study aimed to identify exercises that support balanced
99 activations.

100 **SUBJECTS AND METHOD**

101 The study aimed to determine the electromyographic (EMG) activation of eight muscles of thigh,
102 core/hip, and trunk during common lower extremity exercises in order to provide further
103 knowledge for the development of training, injury prevention, and rehabilitation strategies
104 particularly in athletes at high risk of ACL injuries. The percent of maximum voluntary isometric
105 contractions (MVCs) for each muscle was determined and compared across the five exercises
106 using repeated-measures analysis of variance (ANOVA) in order to determine whether exercise
107 condition had a significant effect on mean activity of each muscle tested.

108 Twelve healthy and physically active female participants with no history of lower extremity or
109 back problems participated in this study in a university research laboratory. Those with a history
110 of lower extremity and low back pain or surgery, neurological disorders, and severe systematic
111 diseases were excluded from the study. The mean age, height, weight and BMI of participants
112 were; 20.10±1.10 years, 165.90±4.77 cm, 63.50±6.22kg, and 23.06 ± 2.17, respectively. The

113 study received ethical approval from the Institutional Review Board and all participants gave
114 written informed consent prior to partaking in the experiments.

115 Five common exercises were performed by each subject; Squat, Sit-Up, Forward Lunge, Glute
116 Bridge, and Double Leg Rise. Subjected performed 10 repetitions of each exercise of 60 beats
117 per minute on a metronome. Participants received instructions as how to perform each exercise:

118 1) Forward Lunge: Participants stood with their feet near each other and hands on their hips, a
119 forward step (with dominant limb) was taken in the sagittal plane and lowering into 90° of hip
120 and knee flexion while the trunk was maintained in an upright position; 2) Squat: Participants
121 stood with feet shoulder-width apart. Hip, knees and ankles were flexed in a squatting motion
122 until reaching 90° of knee flexion (parallel to the horizontal). Participants were instructed to
123 keep their chest up, weight over the heels and not to allow their knees fall into a valgus position;
124 3) Sit-Up: In a supine position on the floor with flexed knees, participants lifted their torso up to
125 approximately 45° at which their torso was in a V position with thighs and then lowered the torso
126 back to the starting position in a controlled manner guided by the metronome; 4) Glute Bridge:
127 Participants laid supine with both knees flexed to 90° and feet flat on the floor. Hips were raised
128 off the floor (pushing through the heels) until a straight line was made between their shoulders
129 and knees. Subjects then lowered their hips back to the starting position in a controlled manor;
130 5) Double Leg Raise: In a supine position with hands by sides or under gluteus (whichever was
131 preferred) and keeping knees in extended position, participants slowly raised both legs until a
132 hip flexion angle of ~75° and held the contraction before lowering both legs according to the
133 metronome.

134 Signal acquisition, processing and analysis were performed using a wireless TeleMyo 2400 G2
135 Telemetry System (Noraxon Inc., Arizona; USA) with synchronised video recording. The
136 bipolar self-adhesive Ag/AgCL surface electrodes (Noraxon Inc., Arizona, USA), with a 20mm
137 inter-electrode distance, were placed in parallel to the muscle fibre orientation²⁰. EMG signals
138 were collected from eight muscles on the dominant side: Vastus Lateralis (VL: two-thirds of the
139 thigh length from the greater trochanter on the lateral side of the thigh), Rectus Femoris (RF:

140 midway between the anterior inferior iliac spine and the patella on the anterior side of the thigh),
141 Vastus Medialis (VM: three-fourths of the thigh length from the anterior inferior iliac spine on
142 the medial side of the thigh), Semitendinosus (ST: midway between the ischial tuberosity and
143 the medial condyle of the femur on the posterior side of the thigh Iliac crest of the right leg),
144 Biceps Femoris (BF: midway between the ischial tuberosity and the lateral condyle of the femur
145 on the posterior side of the thi), Gluteus Maximus (GM: 50% on the line between the sacral
146 vertebrae and the greater trochanter), Erector Spinae (ES: three centimetres lateral to the L3
147 spinous process), and Rectus Abdominis (RA: above the anterior superior iliac spine)^{21,22}.

148 EMG signals from 10 exercise cycles were differentially amplified (Common Mode Rejection
149 Ratio-CMRR>100 dB; input impedance>100 Mohm; gain 500 dB), digitized at a sampling rate
150 of 3000Hz and band-pass filtered at 10-500Hz. This was followed by full-wave rectification and
151 smoothing at 100ms to determine EMG amplitudes by means of root mean square (RMS).
152 Exercise EMG amplitudes were then normalized to the EMG during MVIC for individual
153 muscles: VL- in the sitting position with 90° hip flexion and 90° knee flexion and resistance
154 applied to the distal leg just above the ankle during knee extension; RF- in a sitting position with
155 extended knee and resistance applied to the anterior part of the ankle directed toward the knee
156 flexion; VM- in the sitting position with the knee flexed between 45° to 60° and resistance
157 applied just above the ankle; ST- in a prone position with 90° knee flexion and resistance applied
158 to the posterior part of the ankle in the direction of the knee extension; BF- in a prone position
159 with knee flexion at 45° and resistance applied above the ankle; GM- in the prone position, with
160 the knee flexed to 90° and the hip extended and resistance applied above the knee; ES- in a prone
161 position and resistance applied across the posterior deltoids to resist spinal extension; and RA-
162 a partial curl-up with the feet secured and resistance applied at the shoulders. The maximum
163 EMG signal amplitude (RMS) during the MVIC of each muscle represented 100% muscle
164 activity. The muscle activity recorded during the exercises was then expressed as a percentage
165 of the MVIC and the average amplitudes from 10 exercise repetitions were taken into analysis.

166 A one-way repeated measures analysis of variance (ANOVA) was applied to determine whether
167 exercise conditions had a statistically significant effect on mean EMG activity (%MVIC) of each
168 muscle tested (within exercise differences). Significance was set at the 0.05. A Bonferroni post-
169 hoc test was then applied for the comparative pair-wise analysis of mean normalized EMG (%
170 MVIC) to detect significant differences in the activation of muscles when differences were
171 observed. SPSS (IBM Corp. Released 2013. IBM SPSS Statistics, Version 22.0, NYC) was used
172 for statistical analysis.

173 **RESULTS**

174 Table1 and Figures1-2 summarise and compare the mean activation of muscles during exercises:
175 Forward lunge created significantly higher muscle activation in the VL compared to double leg
176 raise, glute bridge, and sit-up ($p<0.001$). The RF activation was also considerably higher than
177 glute bridge and sit-up ($p<0.001$). Forward lunge generated significantly higher activity in the
178 VM compared to double leg raise and glute bridge ($p<0.05$); and in the BF compared to double
179 leg raise and sit-up ($p<0.05$). Squat was associated with a significantly higher activation in the
180 VL compared to double leg raise, glute bridge and sit-up ($p<0.001$). The RF and VM both were
181 activated significantly higher than glute bridge ($p<0.05$ and $p<0.001$, respectively); and ES had
182 a significantly higher activation compared to double leg raise and forward lunge ($p<0.05$). Glute
183 Bridge produced significantly higher activation in BF and GM compared to double leg raise and
184 sit-up ($p<0.05$); and in the ST compared to double leg raise ($p<0.05$). Sit-Up generated markedly
185 higher activation in the RA ($p<0.001$) compared to forward lunge, glute bridge, and squat; and
186 in the RF compared to glute bridge ($p<0.05$). Double Leg Raise was associated with a
187 significantly higher activation in the RA than in forward lunge, glute bridges and squat
188 ($p<0.001$); and there was a markedly in the RF compared to the glute bridge ($p<0.05$).

189 **DISCUSSION**

190 Findings of this study provide further evidence, by means of muscle activation and
191 strengthening, for optimal prescription of training and rehabilitation exercises in athletes with
192 ACL injury. EMG signal amplitude has been shown to have both linear and non-linear

193 relationship with the force produced by the muscle^{23,24}). and hence, has been widely used to
194 underpin potential rehabilitation exercises by means of enhancing strength, endurance, and
195 stability. It is generally accepted that for strength gains to occur muscle activation should reach
196 the 40% MVC threshold during therapeutic exercises in order to accomplish strengthening
197 adaptation^{25,26}) as such the greater the muscle activation the greater the gains²⁷). The use of
198 exercises with moderate activity, which fail to reach the threshold for strength gains, may instead
199 be used as a high repetition exercise to enhance muscle endurance^{26,28}).

200 One of the strategic aims of the current ACL rehabilitation programmes is to correct aberrant
201 muscle activation patterns of the lower extremity muscles, the quadriceps and hamstrings in
202 particular, following ACL-injury and ACL-reconstruction. These altered activations have been
203 linked to compensatory adaptations in response to arthrogenic muscle inhibition in the
204 quadriceps and/or muscle strength deficits associated with ACL injury (both pre-operatively and
205 following ACL reconstruction)^{10,29}).

206 While the quadriceps function is key for appropriate positioning of the body's centre of mass
207 during communal athletic movements such as running, jump, landings, and cutting
208 manoeuvres³⁰) strong uncontrolled quadriceps forces can lead to anterior translation of the tibia
209 and increase the risk of ACL injury³¹). It is noted that training the quadriceps disproportionately
210 to the hamstrings may impair hamstrings activation, reduce joint stability, increase anterior tibial
211 translation in response to strong quadriceps forces and potentially increase the incidence of ACL
212 injury³⁰). Hence prescribed exercises should have elements of hamstrings training to
213 counterbalance quadriceps activation (restore hamstrings-to-quadriceps activation balance) and
214 support knee ligamentous function in maintaining joint stability and balancing articular surface
215 load distribution³¹).

216 In addition to the lower extremity muscles, the majority of sporting movements also place large
217 demands on trunk/core musculature as they control the body's centre of mass in response to the
218 forces generated from distal body parts^{32,33}). As a result, training of trunk/core muscles should
219 be considered in the training and rehabilitation programmes in order to restore core strength and

220 stability, improve lower extremity alignment, enhance landing quality, and reduce risk of ACL
221 injury by reducing valgus force to the knee^{32,34,35}). Hence, in addition to hamstrings and
222 quadriceps muscles, the present study also measured activity of selected trunk and core muscles,
223 which may directly or indirectly contribute to the knee joint alignment, stability, and mobility,
224 during some commonly prescribed exercises to further support evidence-based training and
225 exercise prescription for the prevention and rehabilitation of ACL injury.

226 The present study found significant differences in the mean activation (i.e. an estimate of
227 exercise intensity) of all muscles across the five exercises indicating their contributions to the
228 potential effectiveness of these rehabilitative exercises. With regard to activation of quadriceps
229 (VL, VM, and RF), forward lunge (32%-61% MVIC) and squat (25%-55% MVIC) appeared to
230 be the optimal exercises and may be considered for enhancing strength and function of this
231 muscle group. This is consistent with that of Ebben et al.³⁶) who reported the highest activation
232 of RF, VL, and VM during squat and forward lunge. Bryanton et al.³⁷) investigated the impact
233 of squat depth on relative muscular effort (RME) and reported increased RME of Knee and hip
234 extensors with greater squat depth. Ayotte et al.²⁵) investigated activation of VM during several
235 weight-bearing exercises and reported considerable activation (sufficient for muscle
236 strengthening) during the wall squat. Ekstrom et al.²⁸) reported activation levels greater than 45%
237 MVIC in the VM during lunge exercises and recommended it for strengthening of the muscle.
238 Pincivero et al.³⁸) also found very high levels of EMG activity for VM and VL during the lunge
239 exercise (150% to 175% MVIC). In terms of different squat exercises, Contreras et al.³⁹)
240 measured mean and peak EMG amplitude of the GM, BF, and VL during front, full, and parallel
241 squats in resistance-trained females and reported similar EMG activity of muscles.

242 Regarding hamstrings, the forward lunge and glute bridge produced considerably higher
243 activation of BF and ST compared to other exercises supporting their integration into the training
244 and rehabilitation programmes for enhancing hamstring function, endurance in particular. It has
245 been shown that hamstrings and ACL act synergistically to limit anterior tibial translation during
246 quadriceps contraction. It has also been suggested that in the presence of ACL injury concurrent

247 increase in hamstring activity and quadriceps inhibition may happen as part of adaptation
248 strategy to resume functional stability⁴⁰). In a study of BF and ST muscle activation during
249 forward lunge, Pincivero et al.³⁸) demonstrated a significant increase in BF activation while no
250 significant increase was found for ST. Ekstrom et al.²⁸) investigated EMG activity of hamstrings
251 during glute bridge exercise and reported a similar activation level of that to the present study.
252 Begalle et al.⁵) reported a very high quadriceps-hamstrings ratio during the lunge exercises.
253 Considering high activity of quadriceps during forward lunge and associated detrimental
254 increase in quadriceps-hamstring activation ratio, the glute bridge may be more advantageous
255 for facilitating a more balanced activation. Farrokhi et al.⁴¹) investigated the effect of changes in
256 trunk position on lower limb muscle activity during forward lunge exercises and found that
257 performing a lunge with a forwarded trunk increased the GM and BF activity compared to when
258 it performed with extended trunk.

259 Emerging data supporting the important role of the muscles acting upon the hip joint, GM in
260 particular, during athletic movements has led to an increasing number of EMG studies aiming
261 to identify optimal training and rehabilitation exercises for athletes with lower extremity
262 injuries^{25,28}). Furthermore, a significant muscle activation deficit has been reported in patients
263 undergoing ACL reconstruction compared to healthy controls⁴²). In the present study GM was
264 activated the greatest during glute bridge (44%MVIC) and forward lunge (40%MVIC)
265 supporting their effective contribution to enhancing core strength and stability. In an EMG study
266 of common exercises, Ekstrom et al.²⁸) reported markedly increased GM activity (36%MVIC)
267 during forward lunge compared to several other exercises and a moderately increased activity
268 during glute bridge (25%MVIC). Some other studies, have however reported significant increase
269 in GM activity during squat-based exercises^{25,43}).

270 The greatest muscle activity for RA and ES was produced during the double leg raise
271 (43%MVIC) and squat (40%MVIC), respectively. While many sporting performances require
272 efficient contribution from the core and trunk muscles for maintaining correct posture and
273 establishing core stability, there is limited data on the activity of RA and ES during lower

274 extremity exercises. As part of lower extremity training and rehabilitation programme, it is
275 critical to maintain the appropriate activity levels and strength of these muscles to enable optimal
276 function and reduce the risk of re-injury. In their study of various core and lower extremity
277 rehabilitation exercises, Ekstrom et al.²⁸⁾ and Comfort et al.⁴⁴⁾ reported the highest RA activity
278 during prone bridge (40%MVIC and 0.454 Root Mean Square-RMS[V] , respectively). These
279 studies did not however include the double leg raise exercise. Comfort et al.⁴⁴⁾ reported a
280 significant increase in the ES activity during front squat (1.010 RMS[V]) suggesting that such
281 dynamic exercise may be beneficial for strengthening the muscle. The study however did not
282 report normalised EMG activity data that would allow direct comparisons.

283 While performing exercises in different planes may influence the kinetics and activation of the
284 muscles, the forward lunge was only measured with the trunk in one plane and squat only to 90°
285 of parallel flexion. Furthermore, study included only two exercises for the true RA activity.
286 Considering emerging evidence to support the employment of more dynamic and criteria-based
287 progression exercises following ACL reconstruction^{45,46)}, some exercises included in the present
288 study such as sit-up and double leg raise may have limited effect on ACL rehabilitation.

289 Findings of this study provide further evidence for optimal prescription of training and
290 rehabilitation exercises in athletes with ACL injury. In terms of muscle activation, study
291 demonstrated that the forward lunge and squat are the best exercises for the quadriceps; the glute
292 bridge and forward lunge for the GM and hamstrings; double leg raise and sit-up for the RA; and
293 squat for the ES. These exercises may be recommended for enhancing muscle activation patterns
294 and muscle endurance. In terms of strengthening (reaching 40%MVIC for strength gain), we
295 recommend squat and forward lunge for the quadriceps, Glute Bridge for the GM, double leg
296 raise for the RA, and squat for the ES. Clinical outcome studies on the efficacy of these exercises
297 in enhancing lower extremity function and in athletes with ACL injury are needed to further
298 support their integration into training and rehabilitation plans.

299 Conflict of interest: None.

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- 419

420 **Table Legends**

421 **Table1.** Comparison of mean (\pm SEM) muscle activation (%MVIC) for individual muscles
422 during five rehabilitation exercises

423 **VL:** Vastus Lateralis; **RF:** Rectus Femoris; **VM:** Vastus Medialis; **BF:** Bicep Femoris; **ST:** Semitendinosus; **RA:**
424 Rectus Abdominis; **GM:** Gluteus Maximus; **ES:** Erector Spinae.

425 *- p<0.05

426 ^a: Significantly higher than Double Leg Raise, ^b: Significantly higher than Forward Lunge; ^c: Significantly higher
427 than Glute Bridge; ^d: Significantly higher than Sit-Up; ^e: Significantly higher than Squat